

## Self-supervised IVIM parameter estimation with a physics based forward model

#### Serge Didenko Vasylechko, Simon K. Warfield, Onur Afacan, Sila Kurugol

Computational Radiology Laboratory, Boston Children's Hospital and Harvard Medical School





$$S(b) = S_0 \left( f e^{-bD^*} + (1-f)e^{-bD} \right)$$

• Intravoxel incoherent motion model (IVIM) is estimated from DWI signal

$$S(b) = S_0 \left( f e^{-bD^*} + (1-f)e^{-bD} \right)$$

• Ill-posed under chinicany reasible acquisition unics

$$S(b) = S_0 \left( f e^{-bD^*} + (1-f)e^{-bD} \right)$$

- Ill-posed under climicany reasible acquisition unics
- e.g. 7 b-values are acquired in ~6-7 minutes

$$S(b) = S_0 \left( f e^{-bD^*} + (1-f)e^{-bD} \right)$$

- Ill-posed under clinicany reasible acquisition unics
- e.g. 7 b-values are acquired in ~6-7 minutes
- Pediatric scanning calls for scan time reduction

$$S(b) = S_0 \left( f e^{-bD^*} + (1-f)e^{-bD} \right)$$

- Ill-posed under clinicany reasible acquisition unics
- e.g. 7 b-values are acquired in  $\sim$ 6-7 minutes
- Pediatric scanning calls for scan time reduction
- Can be achieved with spatial or temporal acceleration

$$S(b) = S_0 \left( f e^{-bD^*} + (1-f)e^{-bD} \right)$$

- Ill-posed under clinicany reasible acquisition unics
- e.g. 7 b-values are acquired in  $\sim$ 6-7 minutes
- Pediatric scanning calls for scan time reduction
- Can be achieved with spatial or temporal acceleration
- Voxelwise NNLS based methods are already very sensitive to noise

$$S(b) = S_0 \left( f e^{-bD^*} + (1-f)e^{-bD} \right)$$

- Ill-posed under clinicany reasible acquisition unics
- e.g. 7 b-values are acquired in ~6-7 minutes
- Pediatric scanning calls for scan time reduction
- Can be achieved with spatial or temporal acceleration
- Voxelwise NNLS based methods are already very sensitive to noise
- No "ground truth" for *supervised* neural network training

# Current remedies to ill-posedness of IVIM estimates

• Spatially constrained methods [1]

[1] Taimouri et al. "Spatially constrained incoherent motion method improves diffusion-weighted MRI signal decay analysis in the liver and spleen", Medical Physics 2015

## **Current remedies to ill-posedness of IVIM estimates**

- Spatially constrained methods [1]
- Bayesian methods [2]

 Taimouri et al. "Spatially constrained incoherent motion method improves diffusion-weighted MRI signal decay analysis in the liver and spleen", Medical Physics 2015
Orton et al. "Improved intravoxel incoherent motion analysis of diffusion weighted imaging by data driven bayesian modeling.", MRM 2014

## Current remedies to ill-posedness of IVIM estimates

- Spatially constrained methods [1]
- Bayesian methods [2]
- Unsupervised (synthetic) voxelwise neural networks [3]

[1] Taimouri et al. "Spatially constrained incoherent motion method improves diffusion-weighted MRI signal decay analysis in the liver and spleen", Medical Physics 2015

[2] Orton et al. "Improved intravoxel incoherent motion analysis of diffusion weighted imaging by data driven bayesian modeling.", MRM 2014[3] Barbieri et al. "Deep learning how to fit an intravoxel incoherent motion model to diffusion-weighted MRI", MRM 2020

• No reference parameter estimates required for training

- No reference parameter estimates required for training
- Data provides supervision via proxy loss

- No reference parameter estimates required for training
- Data provides supervision via proxy loss
- CNNs are inherently robust to noise

- No reference parameter estimates required for training
- Data provides supervision via proxy loss
- CNNs are inherently robust to noise (and fast at test time)

- No reference parameter estimates required for training
- Data provides supervision via proxy loss
- CNNs are inherently robust to noise (and fast at test time)



## Data



- 84 pediatric Crohn's disease patients
- 7 b-values of [0,50,100,200,400,600,800] s/mm<sup>2</sup>
- Geometrically averaged over 6 diffusion gradients

	DW-MRI
Туре	ss EPI
FOV (mm <sup>2</sup> )	300x260
Matrix	192x156
TR / TE (ms)	7500 / 77
Δz (mm)	5
Slices	36-44
NEX	1
Acq. Time (mins)	5.5

## **Evaluation on high SNR data**



[IVIM] Powell et al. "The BOBYQA algorithm for bounded constrained optimization without derivatives.", NA Report 2009 [DeepIVIM] Barbieri et al. "Deep learning how to fit an intravoxel incoherent motion model to diffusion-weighted MRI", MRM 2020

## **Evaluation on high SNR data**



## Evaluation of repeatability on intrasession test-retest



- 6,4,4,3,3 repetitions for 5 healthy volunteers respectively
- 12 voxel ROI

## **Evaluation on data with decreasing SNR**



## Conclusions



- A self-supervised 2D CNN for IVIM parameter estimation
- No ground truth NNLS estimates required
- Increased robustness to low SNR signal
- Enables investigation for reduction of diffusion gradients (& scan time)

### **Questions?**

- serge@crl.med.harvard.edu
- Multicomponent models of diffusion, perfusion and relaxation Wed 19 May, 19:00 UTC

Supported by grants

- NIDDK R21DK123569-01
- NIBIB R21EB029627-01
- NIDDK R01DK125561-01A1
- Soc. of Ped. Rad. & Crohn's & Colitis Found.