# Motion Management in Kidney Diffusion-Weighted MRI

Simon K. Warfield, Ph.D.

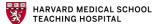
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# Declaration of Financial Interests or Relationships

Speaker Name: Simon K. Warfield, Ph.D.

I have no financial interests or relationships to disclose with regard to the subject matter of this presentation.



# **Motivation for Kidney DWI**

- The kidney is a highly perfused organ with complex anatomy.
  - MRI can reveal morphology, vasculature and function.
- DWI is sensitive to kidney microstructure that changes with maturation, disease and injury:
  - CKD: tubular atrophy, tubular interstation fibrosis
  - Renal ischemia
  - Acute pyelonephritis

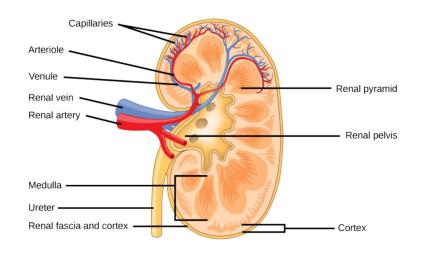
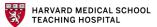


Figure from Chapter 28 of ``Principles of Biology' 2016 by Robert Bear and David Rintoul http://cnx.org/content/m47445/1.4/

- Goal: Improved imaging markers that better characterize microstructure
  - Caroli et al. Nephrol Dial Transplant (2018) doi:10.1093/ndt/gfy163

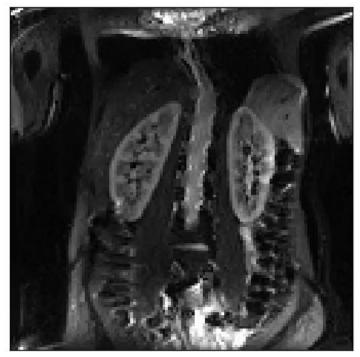




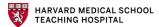


# **DWI for Kidney Imaging**

- DWI contrast is manipulated by changing the diffusion encoding
  - · Diffusion length scale, b-value
  - Orientation of diffusion gradient
- Microstructure from DWI
  - Comparison of signal changes reveals microstructural properties
- Motion can arise from
  - Respiration
  - Cardiac pulsation
  - Bulk motion
    - the subject rolls in the scanner.







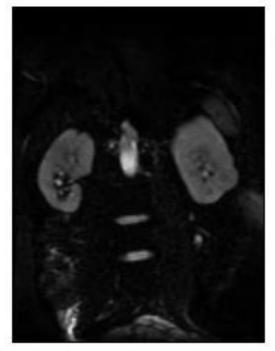


# **DWI for Kidney Imaging: Motion**

- Motion causes the signal from any one voxel in the images to arise from different places in the subject.
  - This reduces the fidelity of parameter estimates of models of the tissue microstructure.
- The DWI signal is measured at different times with varying gradient strengths and orientations.
  - We want to compare the DWI signals arising from the same anatomical location.
- Geometric distortion can also cause misalignment.





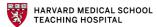




# **DWI for Kidney Imaging: Motion**

- Approaches for motion compensation in renal DW-MRI:
- Navigator triggering, respiratory gating:
  - Acquire data at one instant of the respiratory cycle
  - Don't acquire data at other times in the respiratory cycle
  - Increases scan time (not very practical for routine clinical use)
- Breath holding:
  - Eliminate respiratory motion by not breathing during the scan.
  - Children and subjects who are ill may not be able to breath hold for long.
- We would prefer to continuously acquire DWI during free breathing:
  - Seek to minimize the total scan time
  - Increase patient comfort

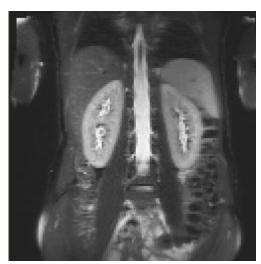






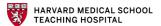
# **DWI for Kidney Imaging**

- Geometric distortion
  - Due to additional phase change during EPI readout due to magnetic susceptibility differences.





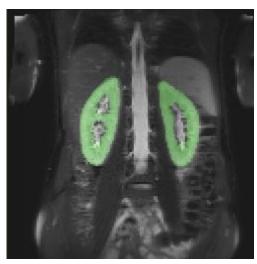


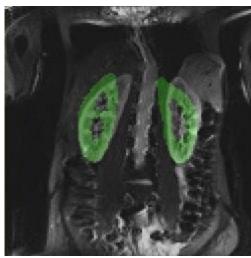




# **DWI for Kidney Imaging**

- Geometric distortion
  - Due to additional phase change during EPI readout due to magnetic susceptibility differences.





- Image acquired with opposite phase encoding direction do not align.
  - Any change in orientation between the static magnetic field and the phase encoding direction alters the geometric distortion.
  - Magnitude of change in distortion depends on the local magnetic susceptibility differences.

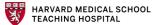




### **Conventional Distortion Correction**

- Measure the distortion field
- Apply correction for the distortion field
- Sequences:
  - PSF mapping
  - Gradient echo sequence to measure phase change
  - Spin echo with phase reversal.

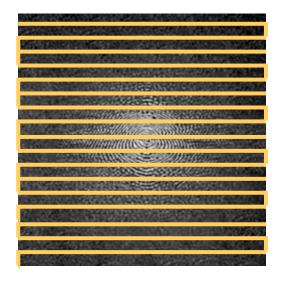






### **Conventional Distortion Correction**

- Measure the distortion field
- Apply correction for the distortion field
- Sequences:
  - PSF mapping
  - Gradient echo sequence to measure phase change
  - Spin echo with phase reversal
    - Acquire two EPI images
      - Opposite phase encoding directions
    - Align the distorted images to measure the magnitude of the change in distortion.
    - Estimate distortion field.



k-space

Coll-Font, J., Afacan, O., Hoge, S., Garg, H., Shashi, K., Marami, B., Gholipour, A., Chow, J., Warfield, S. and Kurugol, S., 2021. Retrospective Distortion and Motion Correction for Free-Breathing DW-MRI of the Kidneys Using Dual-Echo EPI and Slice-to Volume Registration. Journal of Magnetic Resonance Imaging, 53(5), pp.1432-1443.

#### **Problem for Distortion Correction**

- Distortion fields are not static!
  - Breathing moves the tissues and changes the distortion field
  - Pockets of air in the bowel move over time
  - Time to acquire two DWI volumes with opposite phase encoding direction is too long.
    - By the time the second phase encode is acquired, the anatomy has moved to a new position.

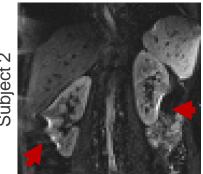
#### Proposed solution:

Acquire two readouts at the same position with opposite phase encoding direction.

EPI readout L->R

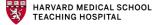






Coll-Font, J., et. al. Journal of Magnetic Resonance Imaging, 53(5), pp.1432-1443.







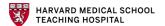
# **Proposed Distortion Correction**

- Modify sequence to obtain images with a dual-echo EPI readout<sup>1</sup>
  - Reverse phase encoding (L->R and R->L) on second readout
  - Very short delay (~40ms) between readouts
  - Assume no motion in between two echos => distortion field is static
- Correct for distortion using L->R and R->L readouts
  - T2 decay between readouts may be non-negligible!
  - Adjust for contrast differences
    - Apply median filter to improve SNR
    - Compensate for amplitude difference
  - Run registration-based distortion compensation<sup>2</sup>

[1] Afacan et al. J. Neurolm 2020. DOI: 10.1111/jon.12708

[2] Hedouin et al. ``Block-Matching Distortion Correction of Echo-Planar Images With Opposite Phase Encoding Directions' IEEE TMI 2017. DOI: 10.1109/TMI.2016.2646920







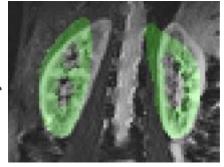
# **Proposed Distortion Correction**

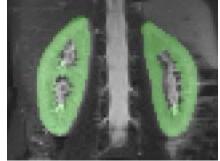
L->R readout

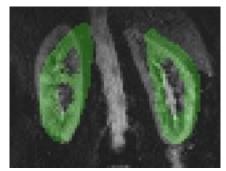
T2 HASTE

R->L readout

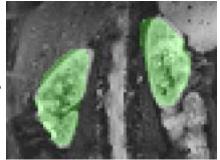




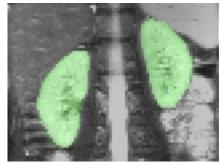




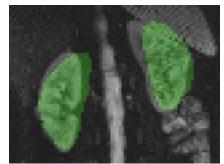
 $\mathcal{C}$ Subject



Distorted



Aligned



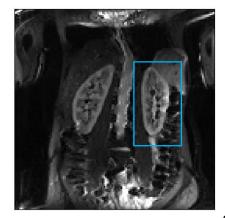
**Distorted** 

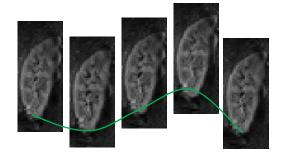




## **Motion Compensation**

- Respiration creates inter-slice motion.
- Slice-to-Volume Registration:
  - Segment each kidney to target organ moving with six degrees of freedom.
  - Motion estimate with registration of each slice to 3D volume.
  - Rigid body motion of kidney with Kalman filter through time.





Kurugol, S. et al., 2017. Motion-robust spatially constrained parameter estimation in renal diffusion-weighted MRI by 3D motion tracking and correction of sequential slices. In Molecular Imaging, Reconstruction and Analysis of Moving Body Organs, and Stroke Imaging and Treatment (pp. 75-85). Springer, Cham.





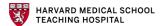
# **Experiments**

- 10 Subjects (ages 29-38, 3 females).
  - Healthy volunteers
  - Acquisition: Imaged with dual-echo DWI sequence
    - 17 directions each with 10 b-values each
  - Analysis pipeline
    - Geometric Distortion Correction of dual echo slices.
    - Slice to volume alignment for motion compensation.
  - For IVIM and DTI models
    - Estimate parameters
    - Leave-one-direction-out cross-validation

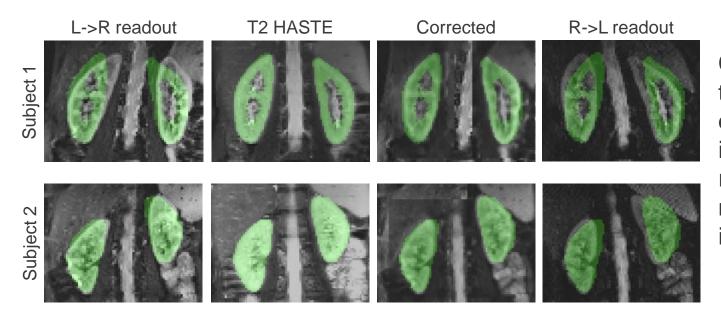
#### **IMAGING PARAMETERS:**

- Dual-echo DWI sequence
- EPI acquisition
  - L->R and R->L phase encoding
- 10 b-values and 17 directions
- 3T Siemens Prisma
- TE1/TE2/TR 72ms/108ms/7000ms
- 18 coronal slices
- Res. 2.81x2.81x4 mm





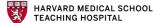
#### Result: Distortion and Motion Correction



Correction for both the geometric distortion of each image and for the respiration induced motion of each image.

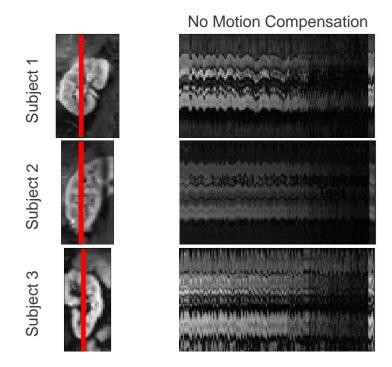
Coll-Font, J., et. al. Journal of Magnetic Resonance Imaging, 53(5), pp.1432-1443.

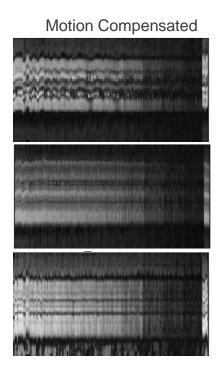






# Result: Slice-to-Volume Registration





Coll-Font, J., et. al. Journal of Magnetic Resonance Imaging, 53(5), pp.1432-1443.







## **Results: Parameter Estimates**

Model param CV (%) /		No correction	DiMoCo
IVIM	Slow diff. (D) [%]	25.7+/-18.3	28.6+/-18.4
	Fast diff. (D*) [%]	63.3+/-21.6	49.6+/-20.5
	Perf. Frac, (f) [%]	38.5+/-14.5	31.4+/-13.7
	nRMSE	0.290+/-0.052	0.154+/-0.056
DTI	MD [%]	8.1+/-1.8	4.3+/-2.6
	FA [%]	14.4+/-1.1	12.4+/-2.4
	nRMSE	0.28+/-0.04	0.12+/-0.01

Correction for distortion and motion leads to:

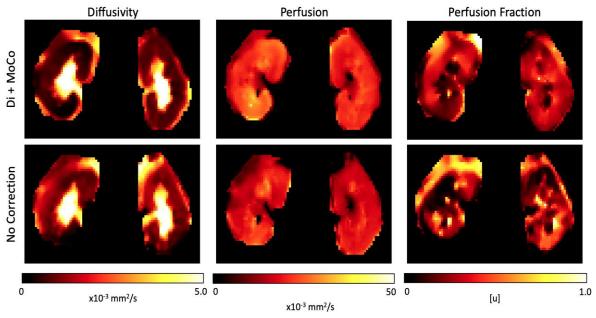
- Reduction in coefficient of variation
- Improved normalized root mean square error.





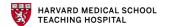


# Results: IVIM parameter maps



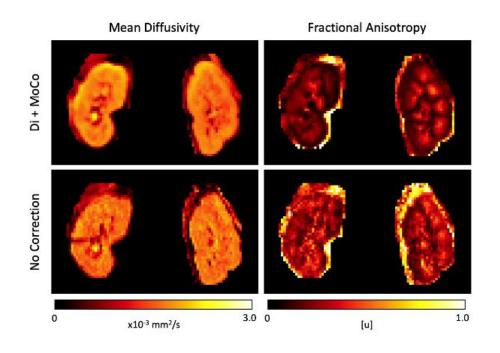
The corrected data leads to improved IVIM parameter estimates.





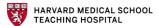


# Results: DTI parameters



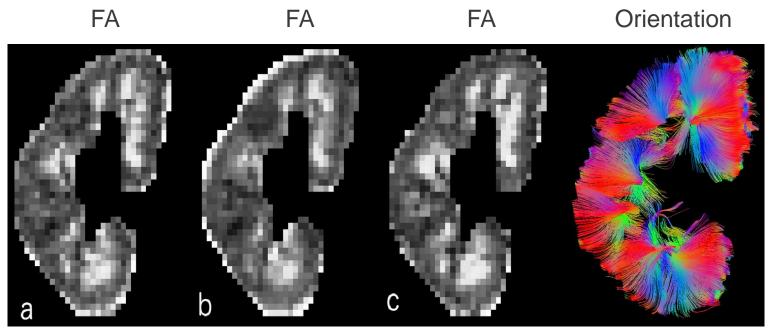
The corrected data leads to improved DTI parameter estimates.





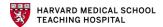


# Results: DTI parameters



No correction Volume alignment. Slice alignment improved orientation visualization.







## **Conclusions and Future Work**

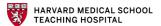
#### Conclusions

- We can correct for distortion despite the presence of motion
  - Enabled by dual echo DWI with polarity reversal for each slice.
- We can correct for respiration induced changes in position.
  - The distortion correction makes it easier to compensate for the respiratory motion.
- These corrections enable DWI to be aligned, increasing the fidelity of parameter estimates for models of tissue microstructure.

#### Future work

- We plan to evaluate the utility of models of kidney microstructure.
  - Reduced influence of the confounds due to motion and distortion.







# Acknowledgements

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  - Jaume Coll-font
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  - Scott Hoge
  - Bahram Marami
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  - Jeanne Chow
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